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### Abstract

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## Fourier-Stokes Polarimetry of Fields Scattered by Birefringent Biological Networks

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**Abstract**—This work presents the results of Stokes vector coordinate distributions determination of biological tissues laser images in Fourier plane. The description of experimental setup – Fourier Stokes-polarimeter is provided. The optical model of polycrystalline networks of histological sections of rectum wall is suggested. The results of investigating the interrelation between the values of statistical (statistical moments of the 1<sup>st</sup>–4<sup>th</sup> order) parameters are presented. They characterize the coordinate distributions of the fourth parameter of Stokes vector of Fourier transforms of laser images of rectum wall histological sections and oncological changes. The diagnostic criteria of rectum cancer are determined.

**Keywords:** polarization, birefringence, anisotropy, phase, laser polarimetry

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### 1. INTRODUCTION

A new direction of optical physical diagnostics [1–8]—laser polarimetry of microscopic images of polycrystalline networks of biological tissues histological sections [9–12] has been developed in recent years. This approach is focused on in vitro measurements of coordinate distributions of Stokes vector parameters of biological tissues laser images with further complex (statistical, correlation, fractal, singular, wavelet, etc.) analysis on the basis of the obtained data arrays [13–24].

Another diagnostic biomedical laser technique—polarizationally sensitive optical coherent tomography—also became widely spread [25–29]. It is based on measuring the parameters of Stokes vector in the remote (Fourier) diffraction zone of the field of scattered laser radiation.

That is why the task of combining the information potentiality of the above mentioned techniques of optical diagnostics basing on the development of new methods of analysis and processing of polarizationally inhomogeneous images of biological tissues in the Fourier plane [30–34] of scattered radiation field proves to be topical.

This research is focused on the development of experimental technique of polarization investigation of coordinate distributions of Stokes vector parameters of the laser field in the Fourier plane for diagnostics and differentiation of the severity of pathological changes in rectum tissue biopsy.

### 2. BASIC ANALYTICAL RELATIONS

It was determined for the fields of scattered laser radiation that polarization state in every point with  $(n, m)$  coordinates is formed by the mechanisms of statistical interference and is determined using the following relations [15, 19, 31]

$$\alpha(n, m) = 0.5 \arcsin \left[ \frac{\sin 2\Theta(n, m)}{\cos \delta(n, m)} \right]; \quad (1)$$

$$\beta(n, m) = 0.5 \arctan \left[ \frac{\sin \delta(n, m)}{\cos 2\Theta(n, m)} \right], \quad (2)$$

where  $\Theta = \arctan \frac{E_y}{E_x}$ —the phase angle,  $\delta$ —phase shift between the orthogonal components  $E_x, E_y$  of

laser radiation amplitude determined from relations [26]

$$E_x e^{i\delta_x} = e^{i\delta_{0x}} E_{0x} \left[ (\cos^2 \rho + e^{-i\phi} \sin^2 \rho) \sin^2 \theta \right] + e^{i\delta_{0y}} E_{0y} \left[ \cos \rho \sin \rho (1 - e^{-i\phi}) \cos^2 \theta \right]; \quad (3)$$

$$E_y e^{i\delta_y} = e^{i\delta_{0x}} E_{0x} \left[ \cos \rho \sin \rho (1 - e^{-i\phi}) \sin^2 \theta \right] + e^{i\delta_{0y}} E_{0y} \left[ (\cos^2 \rho + e^{-i\phi} \sin^2 \rho) \cos^2 \theta \right]. \quad (4)$$

Here  $\delta_{0x}$ ,  $\delta_{0y}$ —phases of orthogonal components ( $E_{0x}$ ,  $E_{0y}$ ) of the amplitude of the laser image probing polycrystalline network;  $\rho$   $\phi$   $\theta$   $\delta = \delta_x - \delta_y = \phi + \theta$ .

Expressions (3) and (4) are “input” parameters for diffraction integrals [31] determining further diffraction-interferential process of evolution of amplitude-phase distributions of object field.

For the case of finding the biological tissue layer in the focal plane of the objective the following can be written

$$U_x(m^*, n^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_x(m, n) \exp \left[ -i \frac{2\pi}{\lambda f} (nn^* + mm^*) \right] dndm; \quad (5)$$

$$U_y(m^*, n^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_y(m, n) \exp \left[ -i \frac{2\pi}{\lambda f} (nn^* + mm^*) \right] dndm. \quad (6)$$

Here  $f$ —focus distance of the objective;  $\lambda$ —wave length of laser radiation;  $n$ ,  $m$  and  $n^*$ ,  $m^*$ —coordinates of the points in the image plane and Fourier plane respectively.

Diffraction integrals (5) and (6) enable to determine the asymmetry degree of Fourier spectrum in two mutually transverse directions

$$\Delta(v) = \frac{U_x(m^*) + U_y(m^*)}{U_x(n^*) + U_y(n^*)}, \quad (7)$$

where

$$U_x(m^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_x(m) \exp \left[ -i \frac{2\pi}{\lambda f} mm^* \right] dm = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_x(m) \exp[-i2\pi m v_m] dm; \quad (9)$$

$$U_x(n^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_x(m) \exp \left[ -i \frac{2\pi}{\lambda f} nn^* \right] dn = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_x(m) \exp[-i2\pi n v_n] dn; \quad (10)$$

$$U_y(m^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_y(m) \exp \left[ -i \frac{2\pi}{\lambda f} mm^* \right] dm = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_y(m) \exp[-i2\pi m v_m] dm; \quad (11)$$

$$U_y(n^*) = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_y(n) \exp \left[ -i \frac{2\pi}{\lambda f} nn^* \right] dn = \frac{A}{i\lambda f} \int_{-\infty}^{+\infty} E_y(n) \exp[-i2\pi n v_n] dn. \quad (12)$$

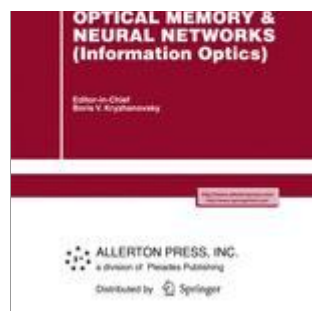
Thus, taking into account relations (1)–(6) the following expressions for the Stokes vector parameters can be written [32]

$$\begin{aligned} S_1(m^*, n^*) &= E_x E_x^* + E_y E_y^*; \\ S_2(m^*, n^*) &= E_x E_x^* - E_y E_y^*; \\ S_3(m^*, n^*) &= E_x E_y^* - E_y E_x^*; \\ S_4(m^*, n^*) &= i(E_y E_x^* - E_x E_y^*), \end{aligned} \quad (13)$$

and asymmetry degree of  $S_{k=1,2,3,4}(m^*, n^*)$  distributions can help to determine the degree of asymmetry (relations (7)–(12)).

For objective (quantitative) estimation of distributions  $S_{k=1,2,3,4}(m^*, n^*)$  the statistical, correlation and spectral approaches were used.





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